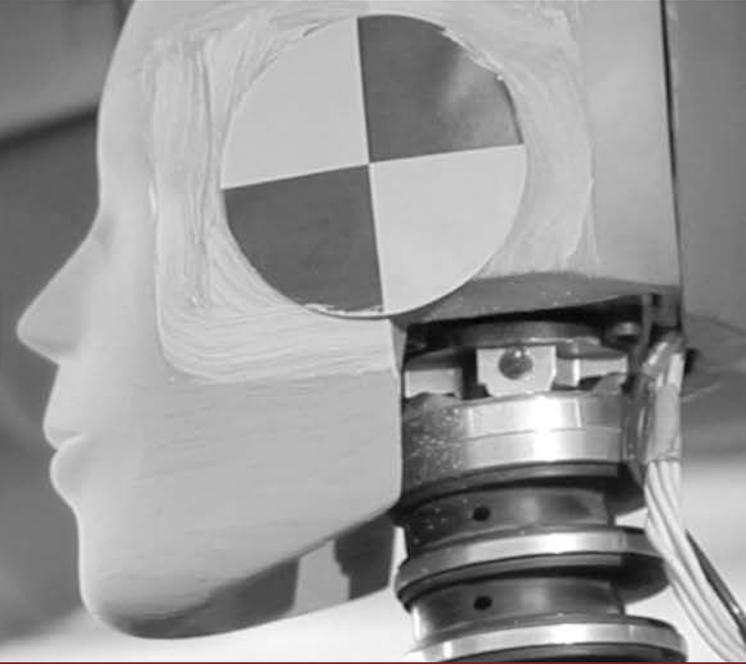


# Development of the Large Omnidirectional Child (LODC) ATD



Jason Stammen (NHTSA)

Brian Suntay (TRC)

Mike Carlson, Yun-Seok Kang (OSU)

SAE Government/Industry Meeting

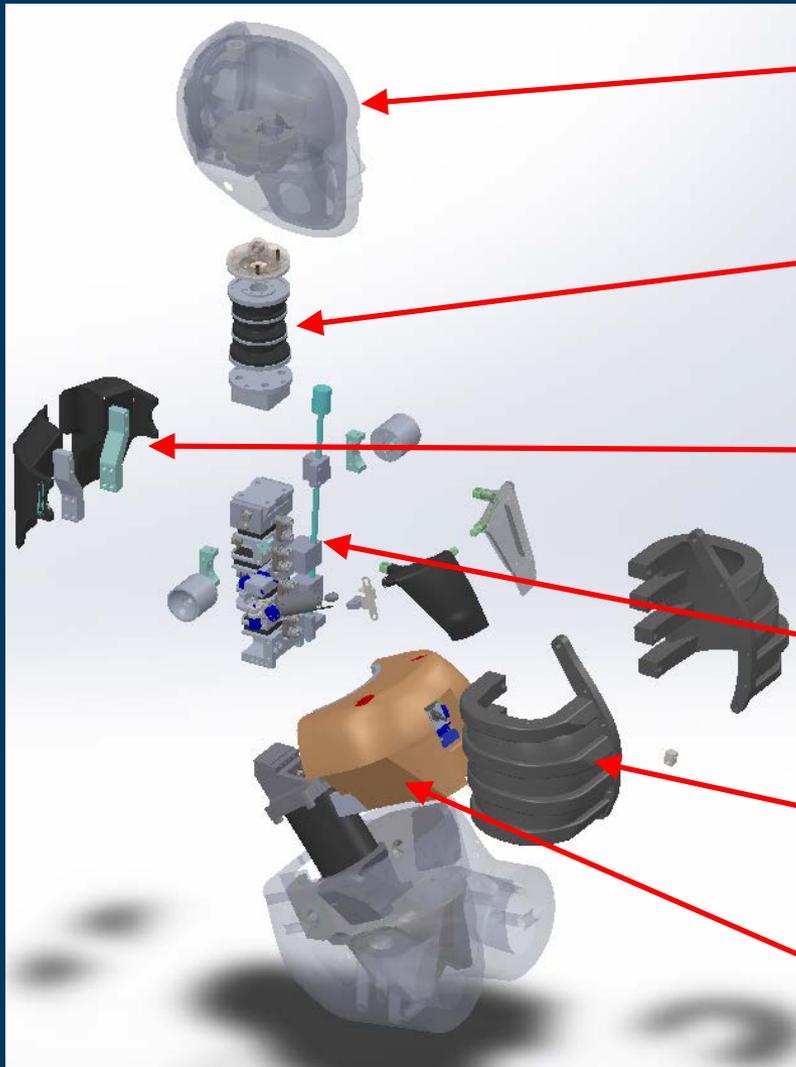
January 21, 2016

# Motivation

- Improvements to Hybrid III child ATD performance needed
  - Head kinematics & neck loads
  - Abdomen injury assessment
  - Belt interaction with thorax & shoulder
- Large Omnidirectional Child (LODC)
  - 10YO size
- Prototype development activities done in-house



# LODC: Design Overview



Head mass properties adjusted to Duke human head data

Neck assembly tuned to Duke pediatric model response

Shoulder will carry shoulder belt loads in a humanlike way

Flexible thoracic spine tuned to human data

Ribcage tuned to 10 year old human corridor

Abdomen instrumentation to measure injury risk

# Head: Design

LODC head should have proper mass properties & respond correctly in impact



Measurement	10YO Human	LODC	Hybrid III 10YO
Mass (kg)	3.56	3.56	3.73
CG to OC (x, mm)*	17.8	18.6	20.1
CG to OC (z, mm)	52.8	52.5	44.8
Ixx (mm <sup>4</sup> )	0.0121 ± 0.0014	0.0118	0.0120
Iyy (mm <sup>4</sup> )	0.0150 ± 0.0014	0.0153	0.0160
Izz (mm <sup>4</sup> )	0.0112 ± 0.0008	0.0118	0.0130

Human properties from Loyd et al. (Stapp 2009)

\*CG-OC(x) was weakly correlated with characteristic length, so linear interpolation alone between 9-16YO specimens was used for human target

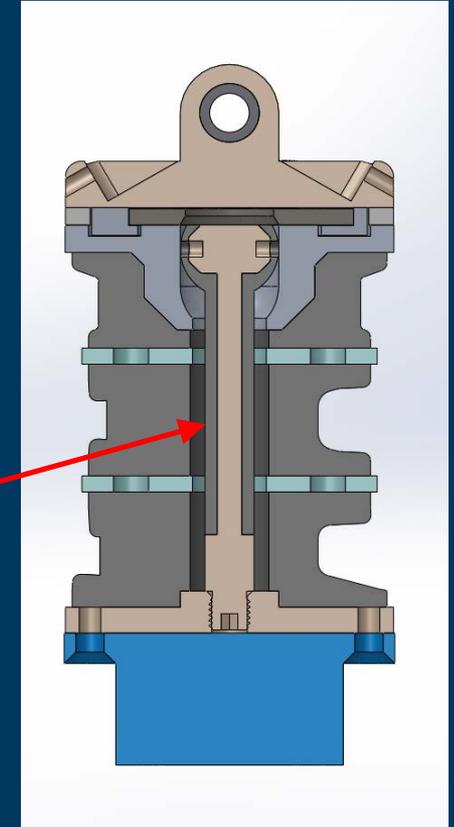
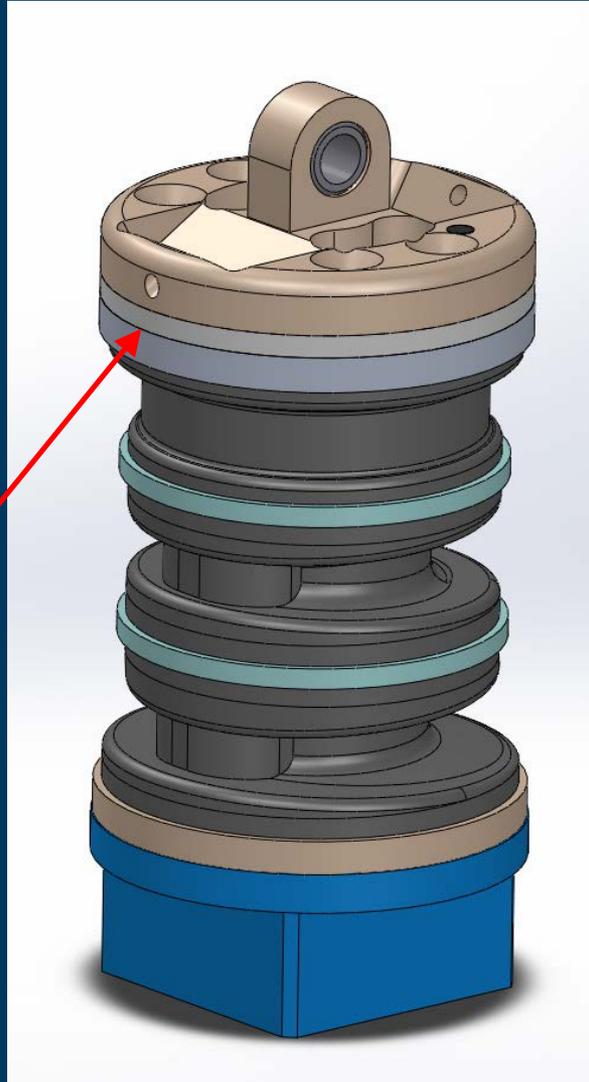
- Secondary focus: revise head skin to match head drop response targets from Loyd et al (2009)

# Neck: Design

20 degrees free range of motion in Z-axis

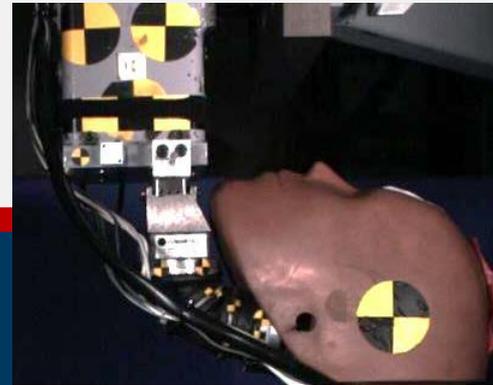


C2 twist mechanism for more humanlike off-axis ROM

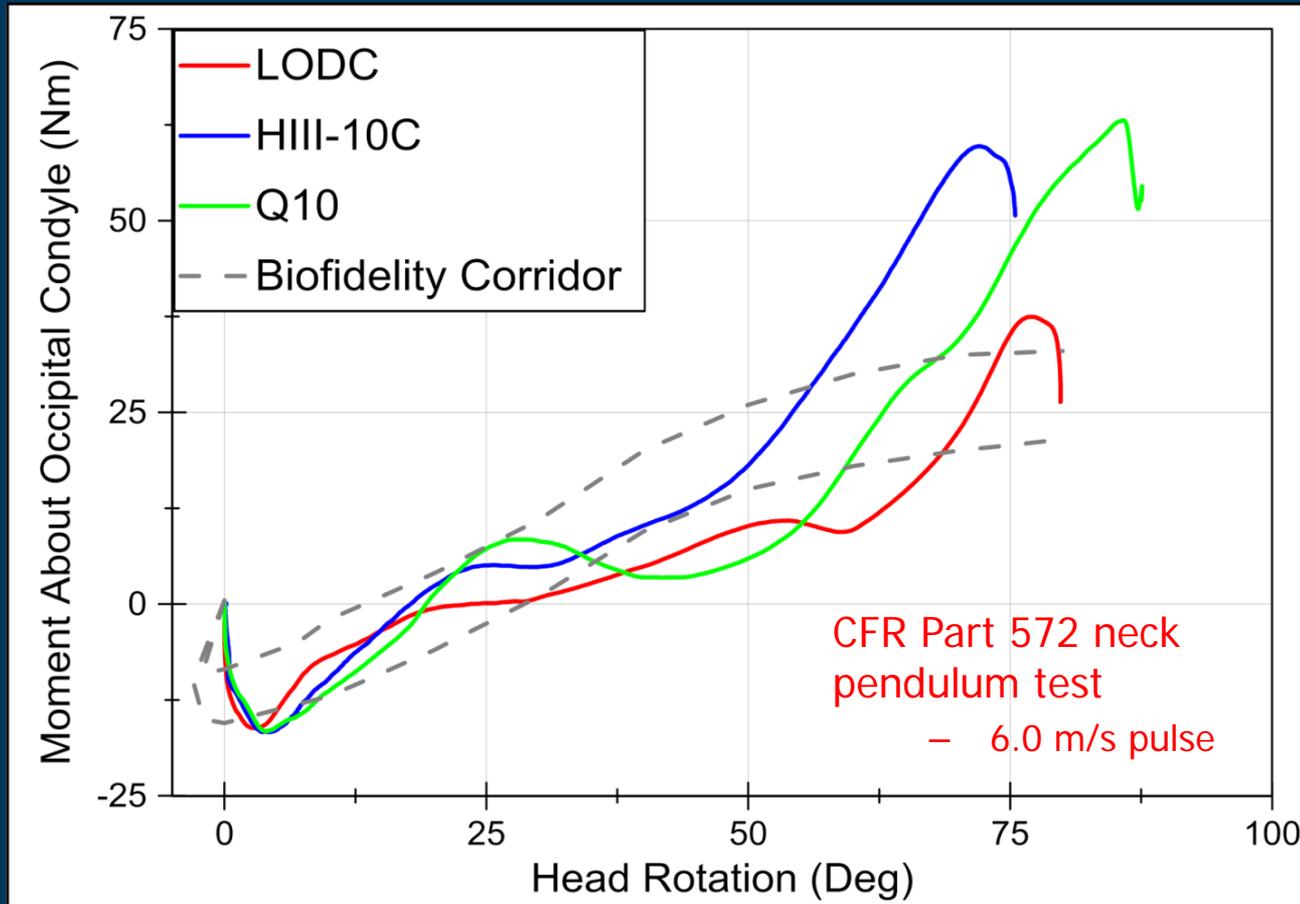


Over-molded central cable that allows some elongation without fasteners, reducing risk of interference & noise

# Neck: Response



Biofidelity Target From Dibb et al (ESV 2013)



# Thoracic Spine: Design

Flexible, stable, and repeatable

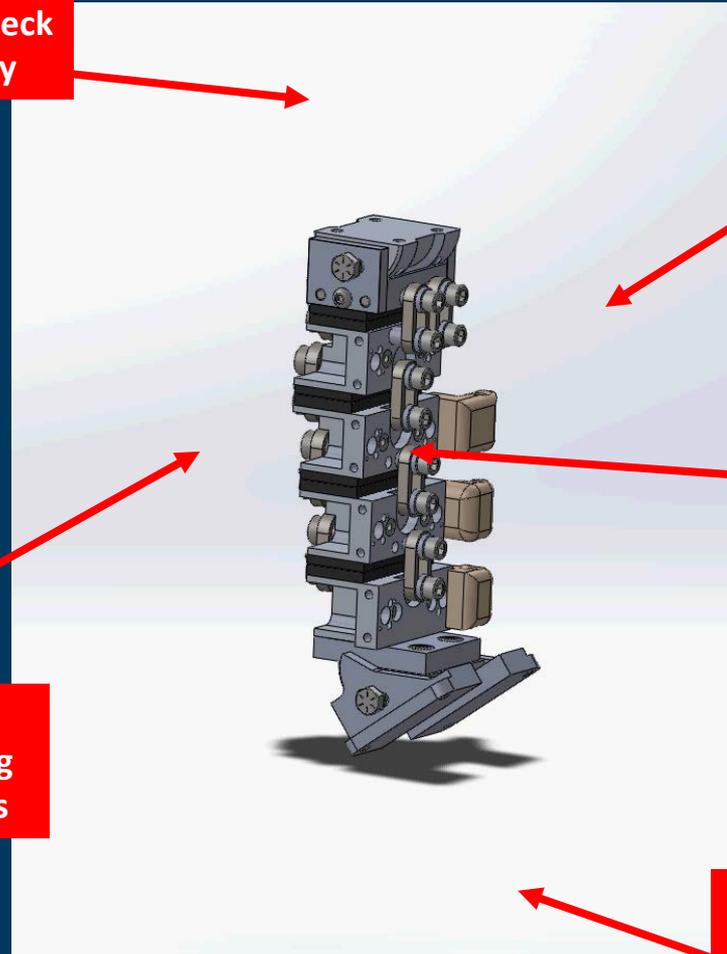
Angle adjustment at lower neck adds positioning versatility

Top thoracic joint has two anterior links for added stability during seating

Thoracic mounts provide posterior rib and shoulder attachment, and mounting locations for motion blocks to measure spine motion

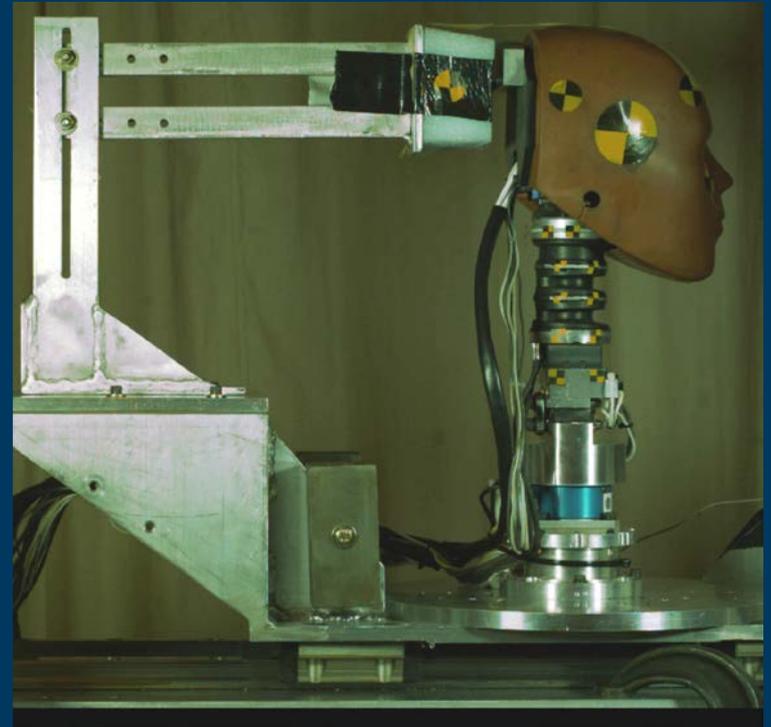
Bi-layer rubber elements provide flexibility while being stabilized by connecting links

Lumbar bracket is adjustable within the range of normal child seated postures



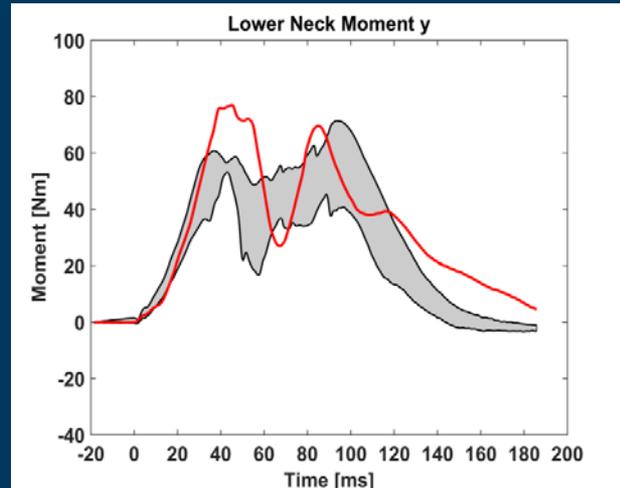
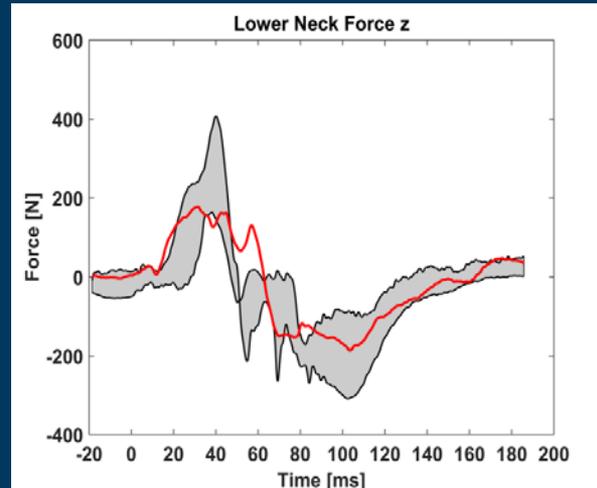
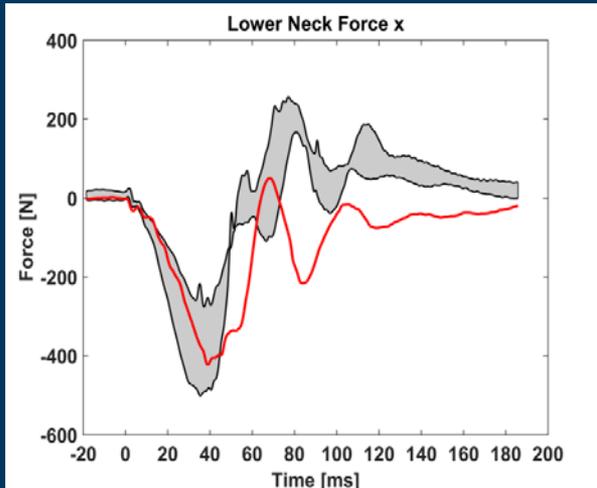
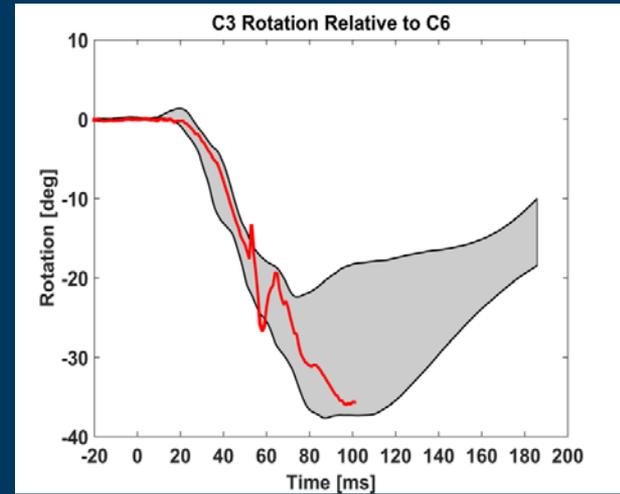
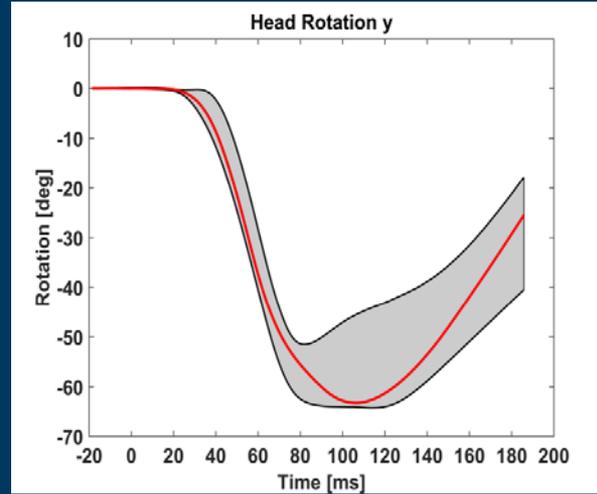
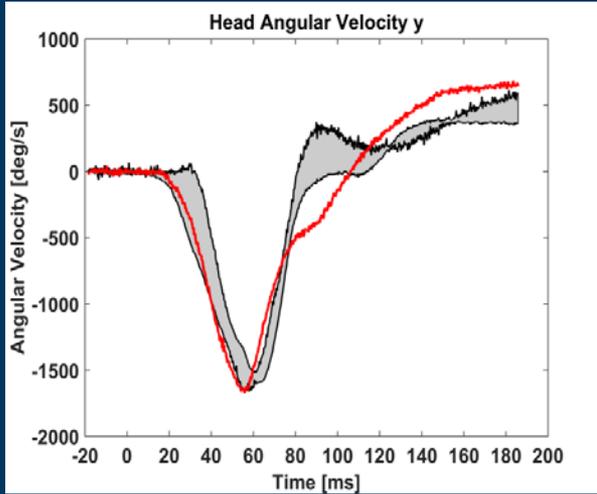
# Cervicothoracic Spine: Test Setup

- **Goal:** Exercise neck and upper spine together in flexion
- **Pulse:** 12 G, 4 m/s (based on T1 X acceleration data from a FMVSS No. 213 sled test)
- **Biomechanical reference:** Adult PMHS scaled to LODC size (Kang et al 2016, in progress)



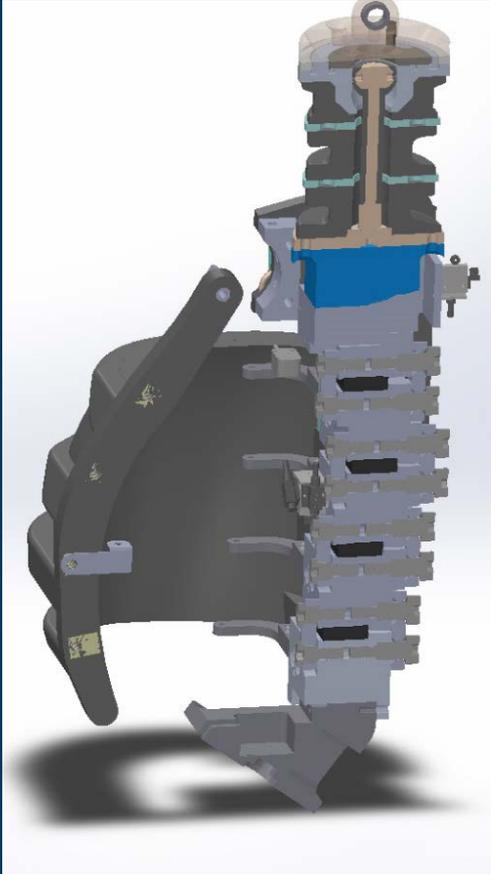
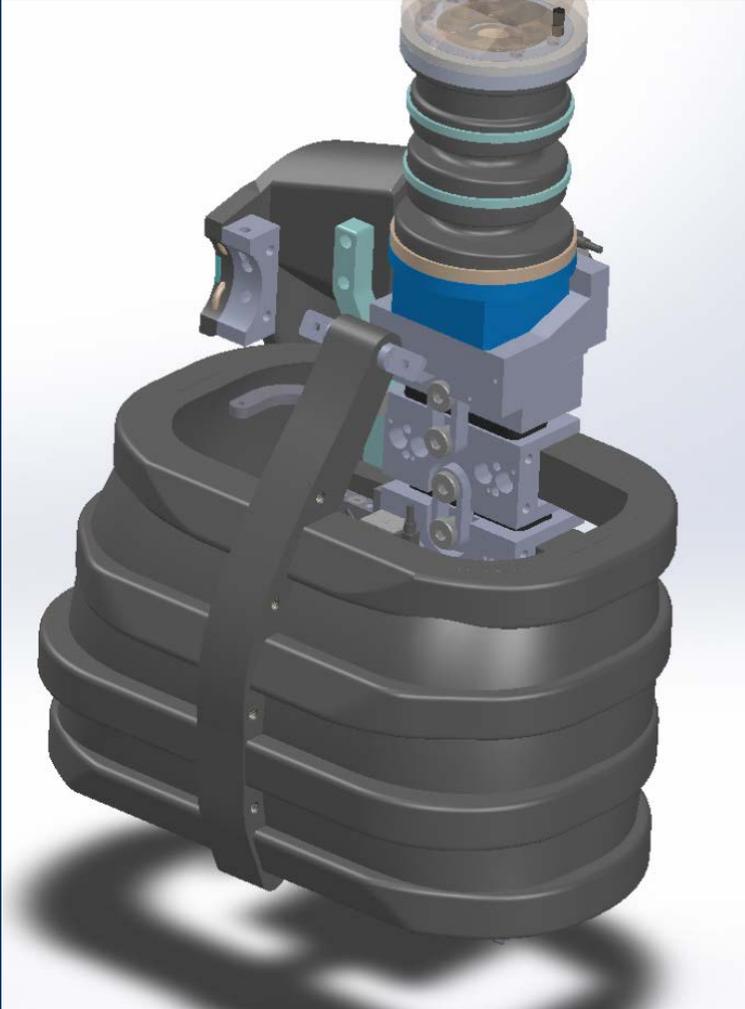
# Thoracic Spine: Response

LODC should display proper head kinematics and neck loads



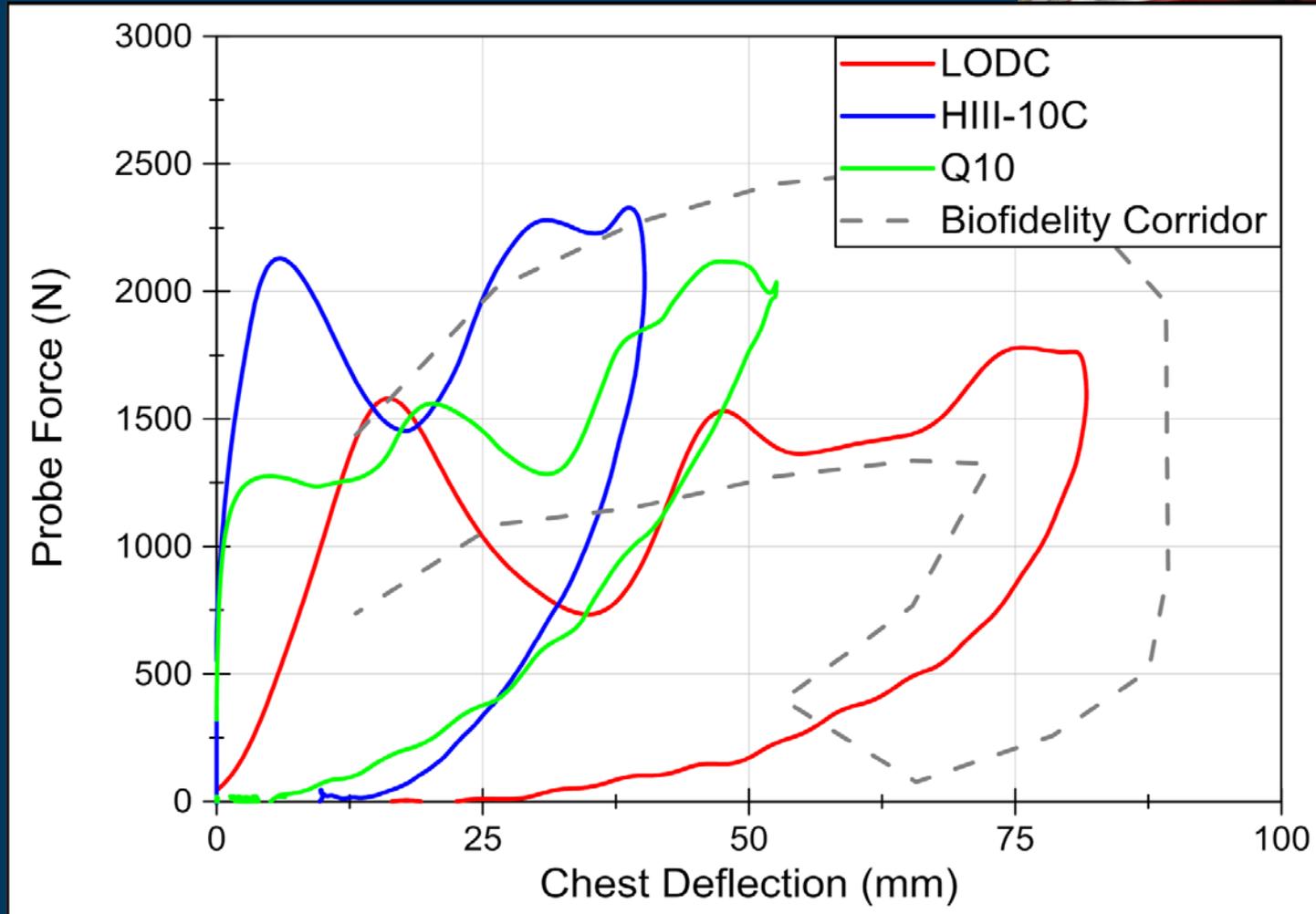
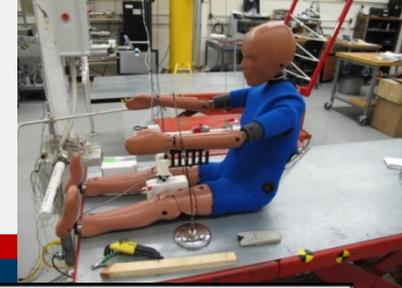
# Thorax: Design

Two hemispheres with continuous interior surface to maintain rib alignment



# Thorax: Response

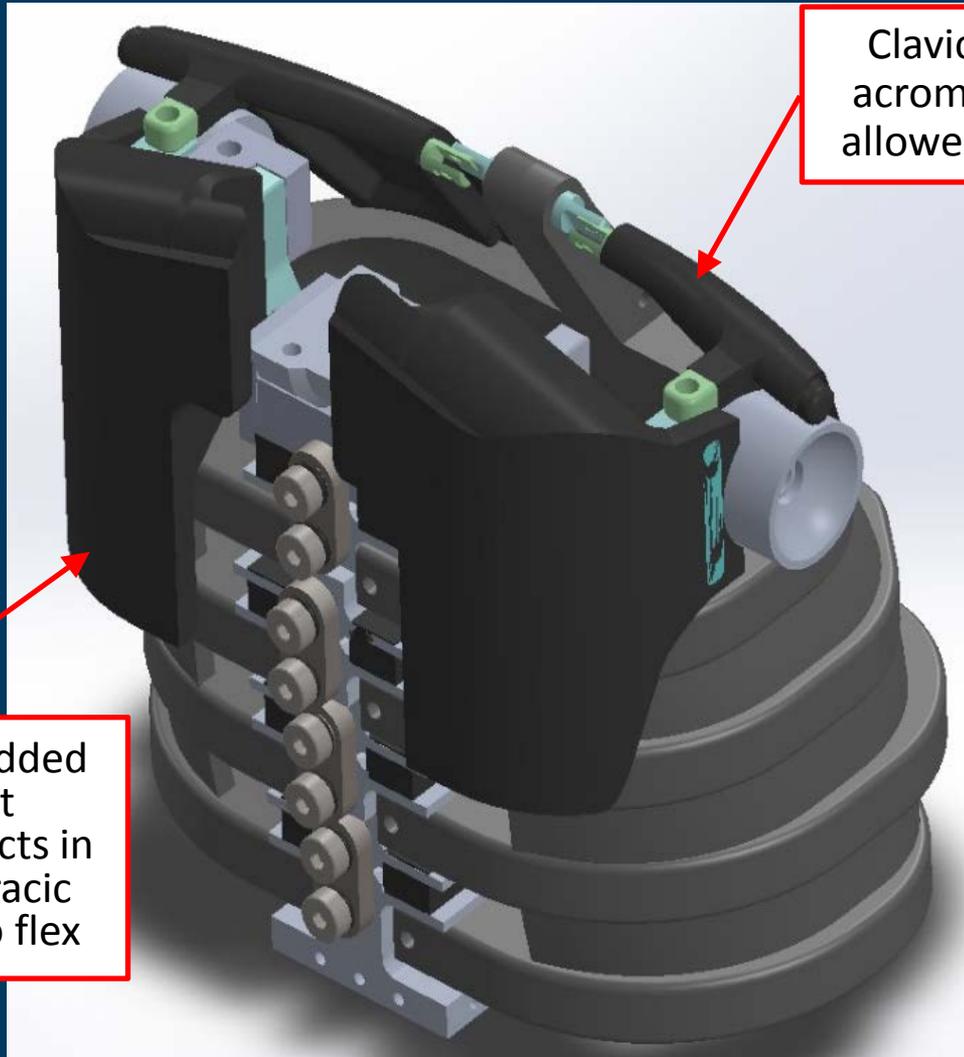
Tune LODC thorax stiffness to reflect human response



Biofidelity Target derived by Parent et al (2010) from Ouyang et al (2006) data

# Shoulder: Design

Humanlike construction with clavicle-acromion-scapula load path to the spine

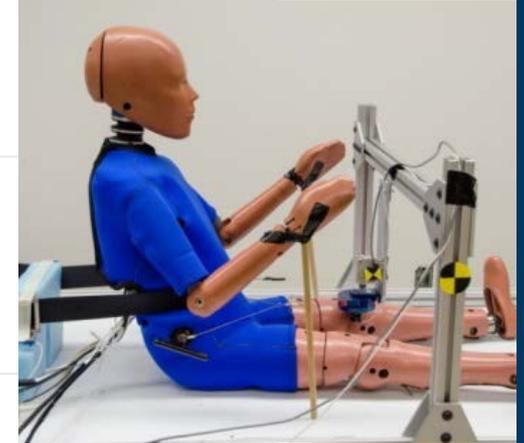
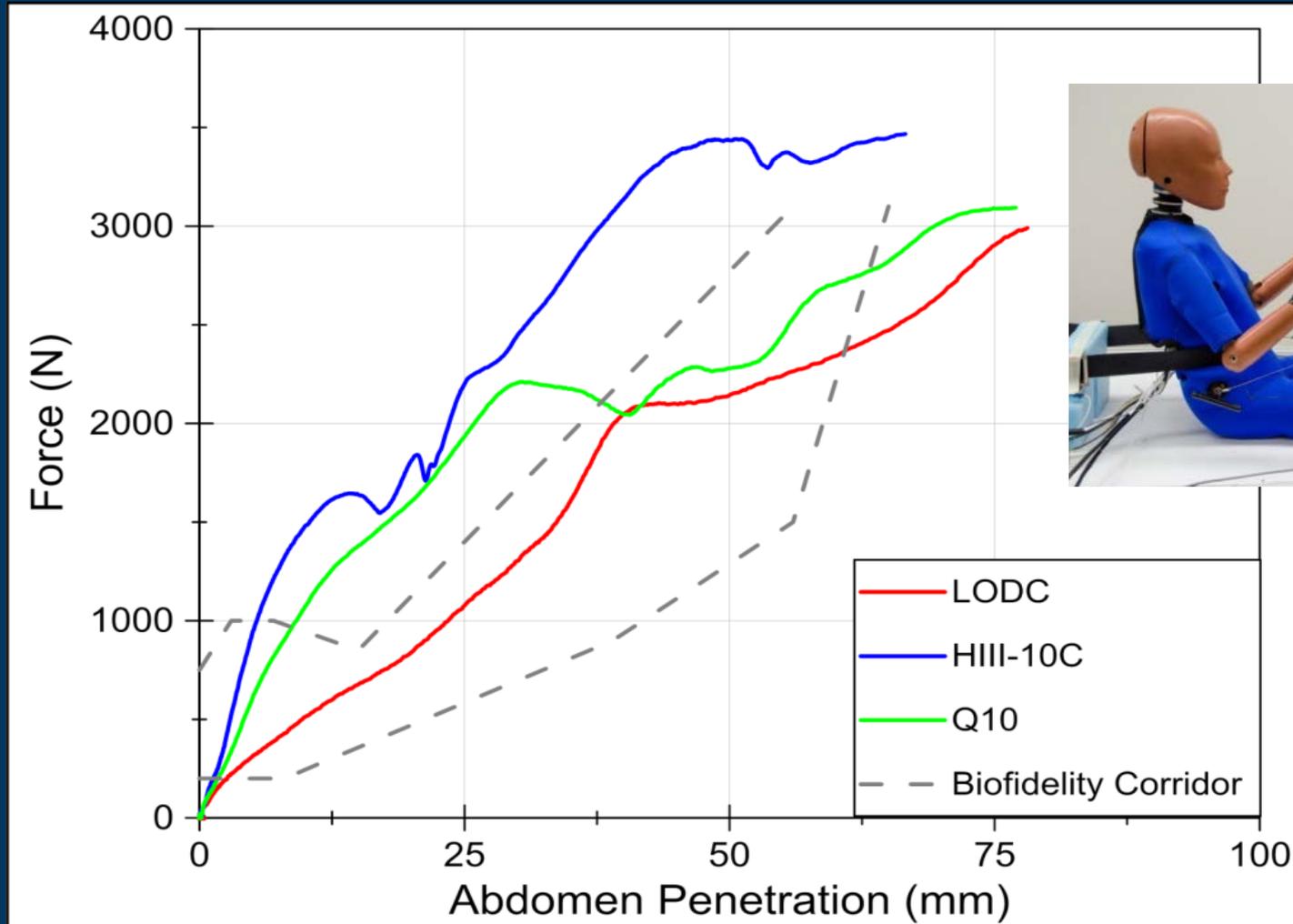


Clavicle connects sternum to acromion with relative motion allowed at SC and AC joint ends

Scapula provides added support for belt resistance & connects in a way so that thoracic spine is still free to flex

# Abdomen: Response

Same geometry as Hybrid III 10YO but heavier and softer; pelvis same as Hybrid III



Biofidelity Targets From Kent et al (Stapp 2008)

# Full Dummy Evaluation

Compare with Hybrid III 10YO in FMVSS No. 213 condition. Does LODC:

- Replicate the head kinematic trajectory characteristics of previously conducted pediatric PMHS/volunteer testing?
- Eliminate chin-chest induced head acceleration spikes?
- Reduce neck loads to levels more suitable for neck injury risk assessment?
- Provide added sensitivity for distinguishing between restraint conditions?
- Identify the potential for submarining and measure abdominal injury risk?

# Full Dummy Evaluation

Visual comparison with Hybrid III 10C ATD

## 5-PT HARNESS



Hybrid III 10YO



LODCrev2

## BACKLESS BOOSTER



Hybrid III 10YO



LODCrev2

## HIGHBACK BOOSTER



Hybrid III 10YO



LODCrev2

## NO CRS



Hybrid III 10YO



LODCrev2

\*For more details on the upgraded 213 bench, see [NHTSA-2013-0055-0002](https://www.nhtsa.gov/document/2013-0055-0002)

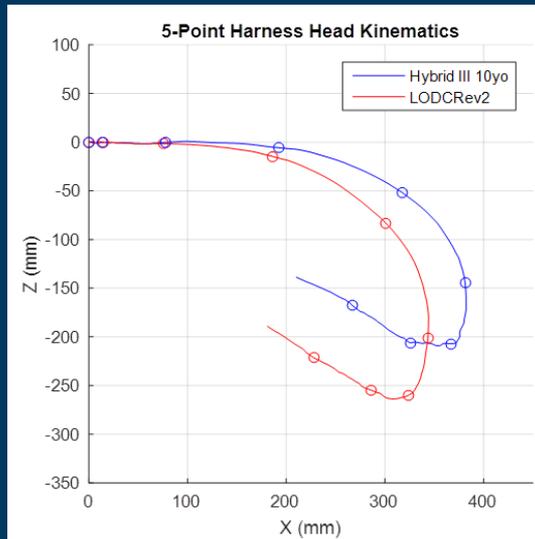
*Safer drivers. Safer cars. Safer roads.*

# Full Dummy Evaluation

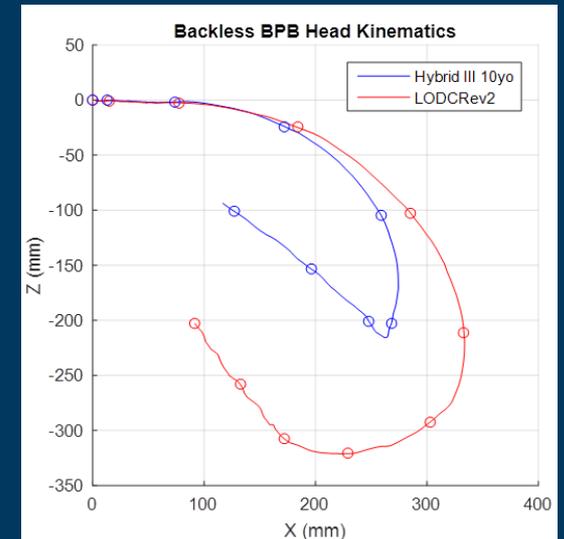
Head/spine trajectories more reflective of human data (more X & Z translation)



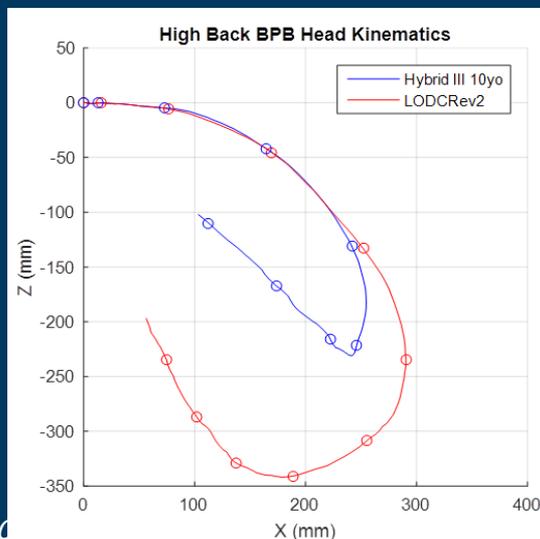
**5-PT HARNESS**



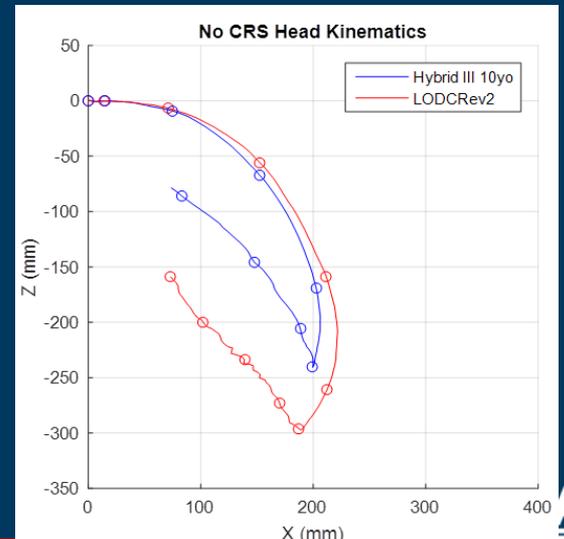
**BACKLESS BOOSTER**



**HIGHBACK BOOSTER**

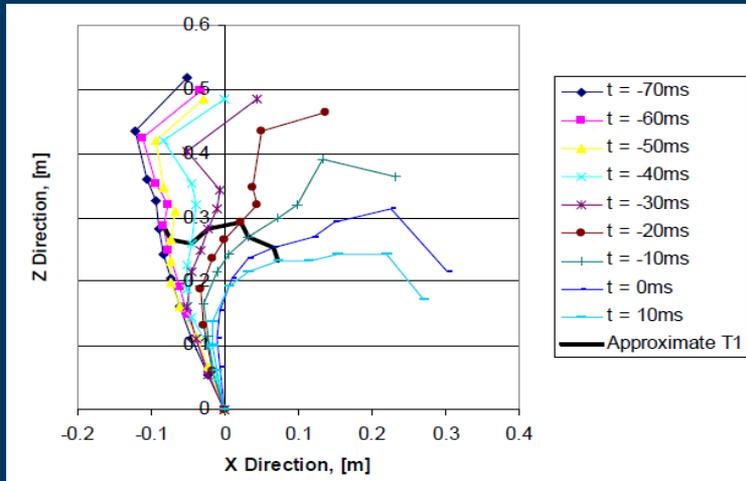


**NO CRS**

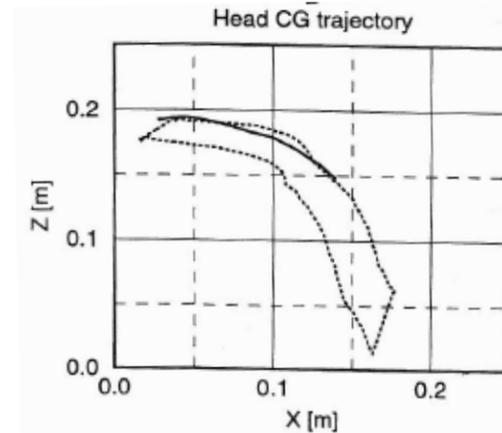


# Full Dummy Evaluation

Head/spine trajectories more reflective of human data (ratio of Z to X peak displacement)



Ash et al 2009: Re-analyzed 13YO PMHS data from Kallieris et al 1976 showed roughly 1:1 ratio of peak X/peak Z head CG displacement

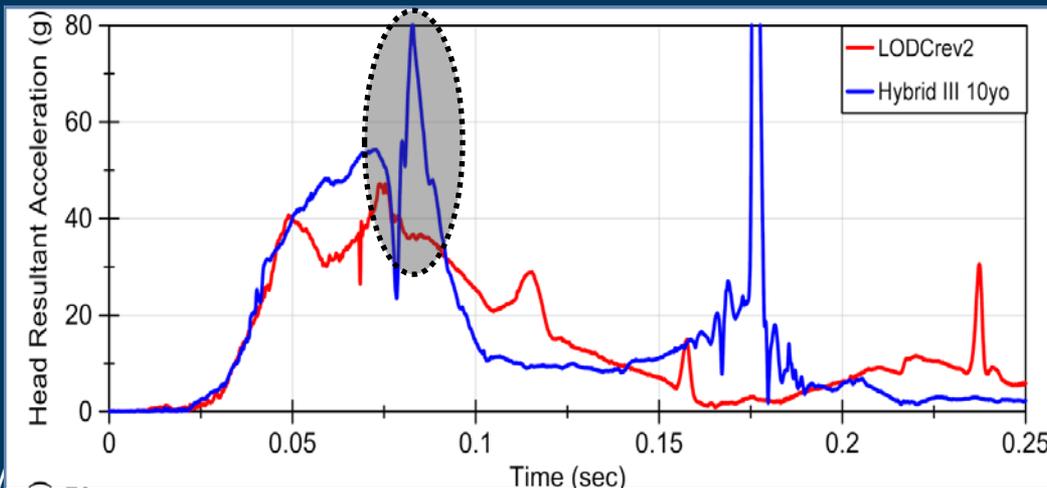


Thunnissen et al 1995: adult volunteers had significantly greater Z (vertical) displacement for head CG than Hybrid III 50<sup>th</sup> ATD did

Restraint	$Z_{\text{peak}} / X_{\text{peak}}$ (Hybrid III 10YO)	$Z_{\text{peak}} / X_{\text{peak}}$ (LODC)
5 Pt Harness	0.54 <	0.77
Highback BPB	0.88 <	1.17
Backless BPB	0.77 <	0.98
No CRS	1.20 <	1.34

# Full Dummy Evaluation

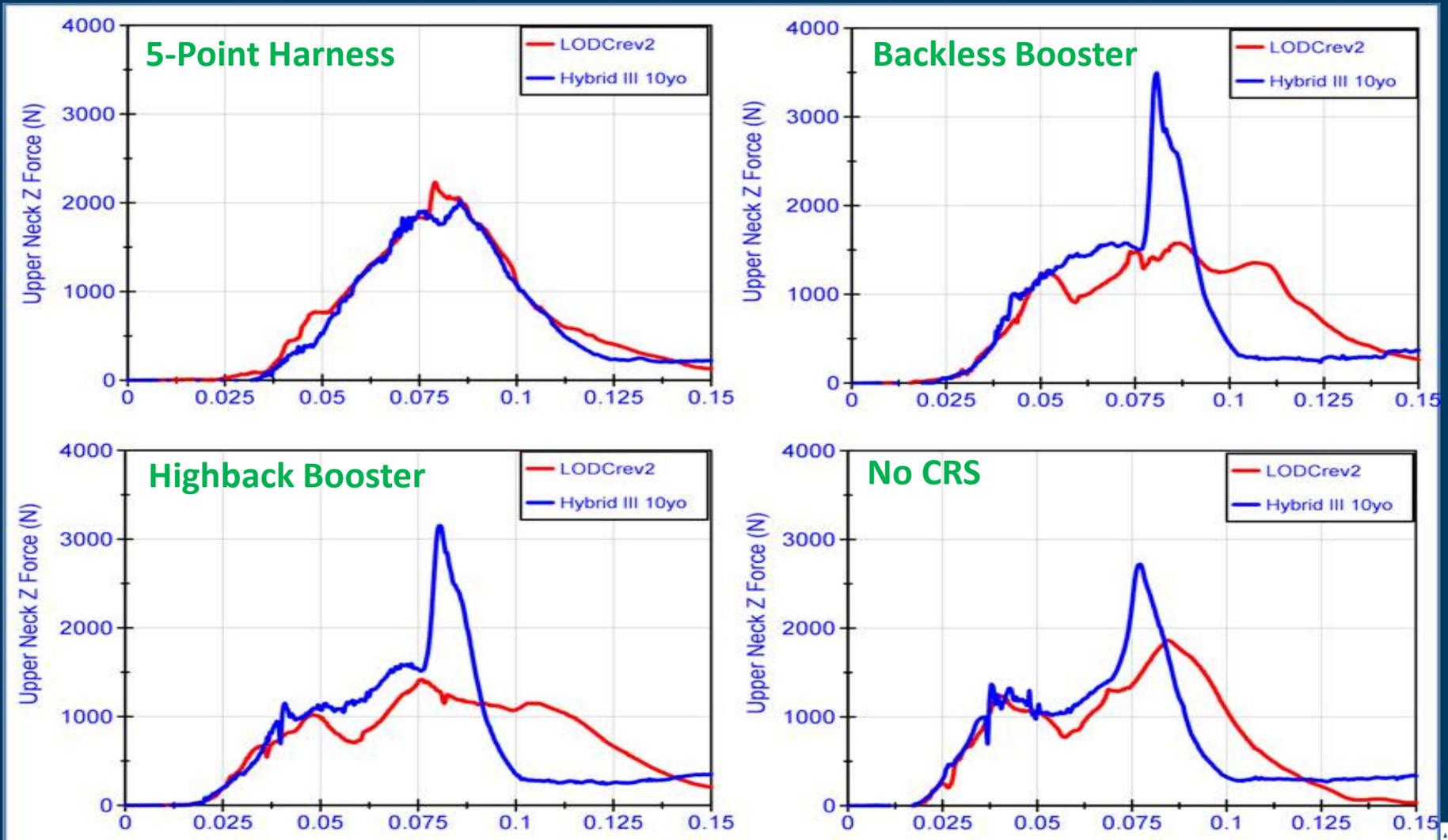
Eliminates head acceleration spikes (& high HIC) induced from chin-chest contact



CRS	ATD	HIC36
5-pt Harness	LODC	481
	H3	497
High Back	LODC	214
	H3	531
Backless	LODC	306
	H3	1956
No CRS	LODC	271
	H3	637

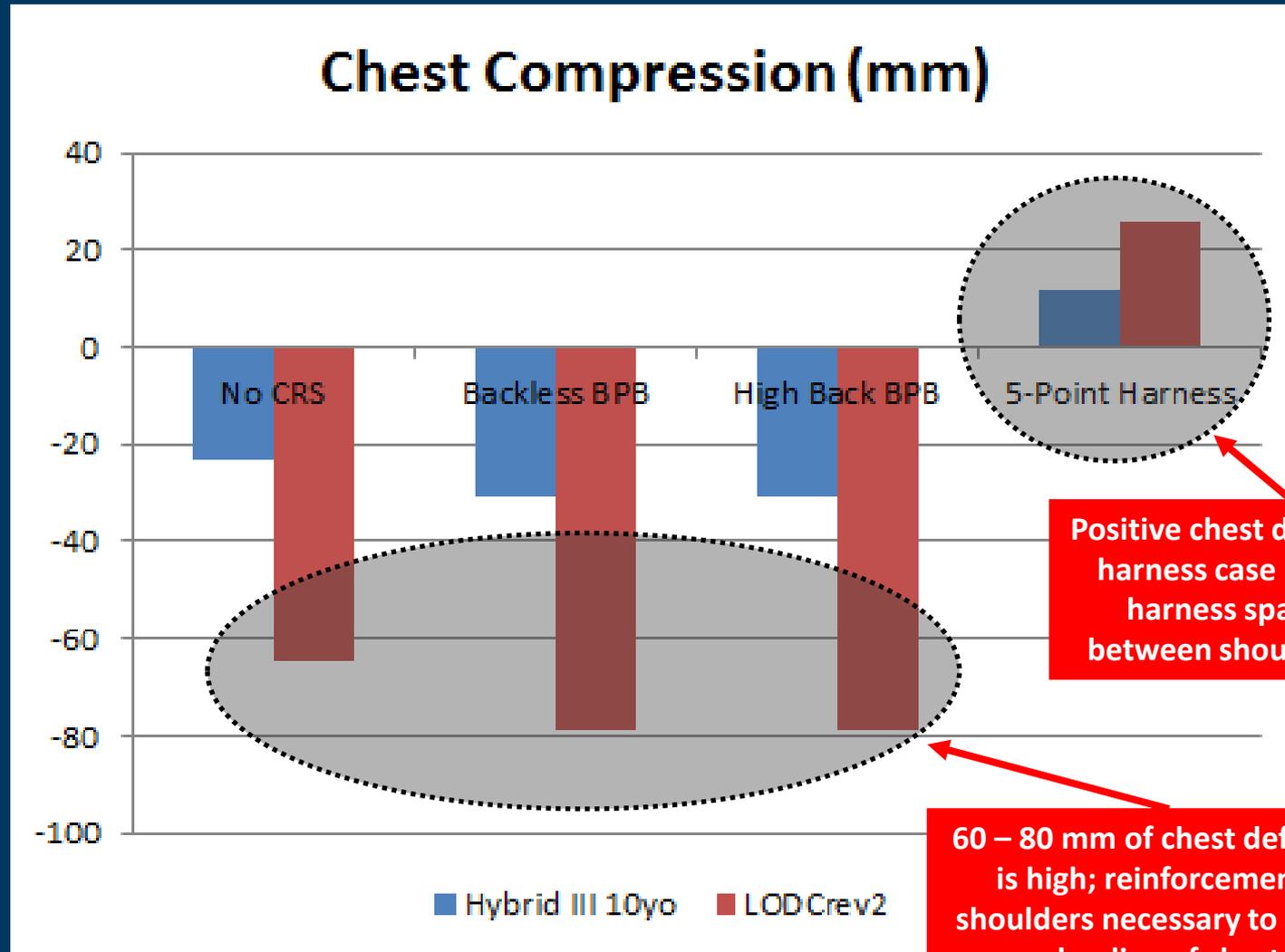
# Full Dummy Evaluation

Reduced neck tensions to levels more appropriate for neck injury assessment



# Full Dummy Evaluation

Large chest compressions?

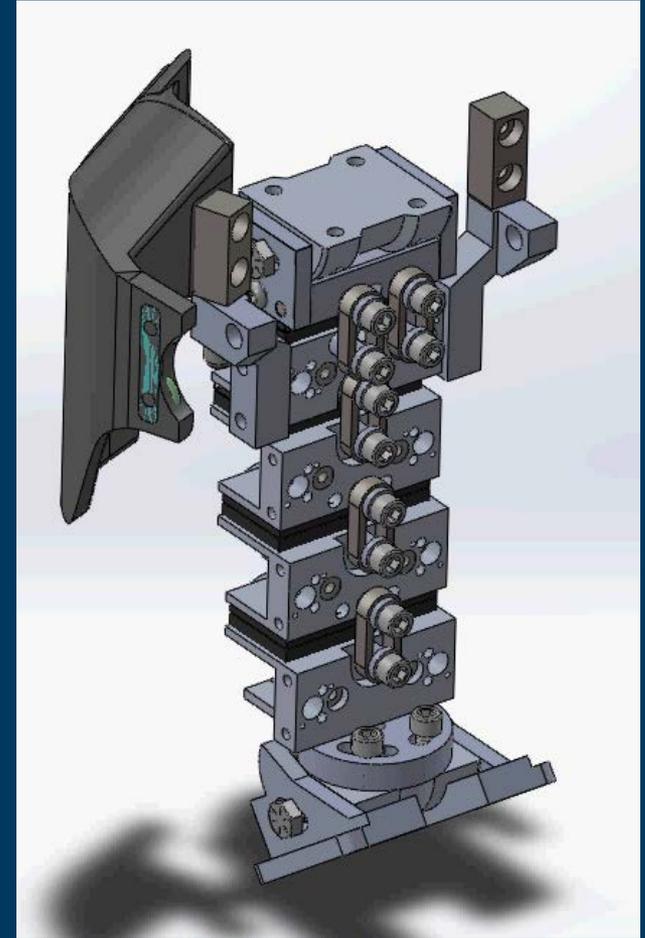
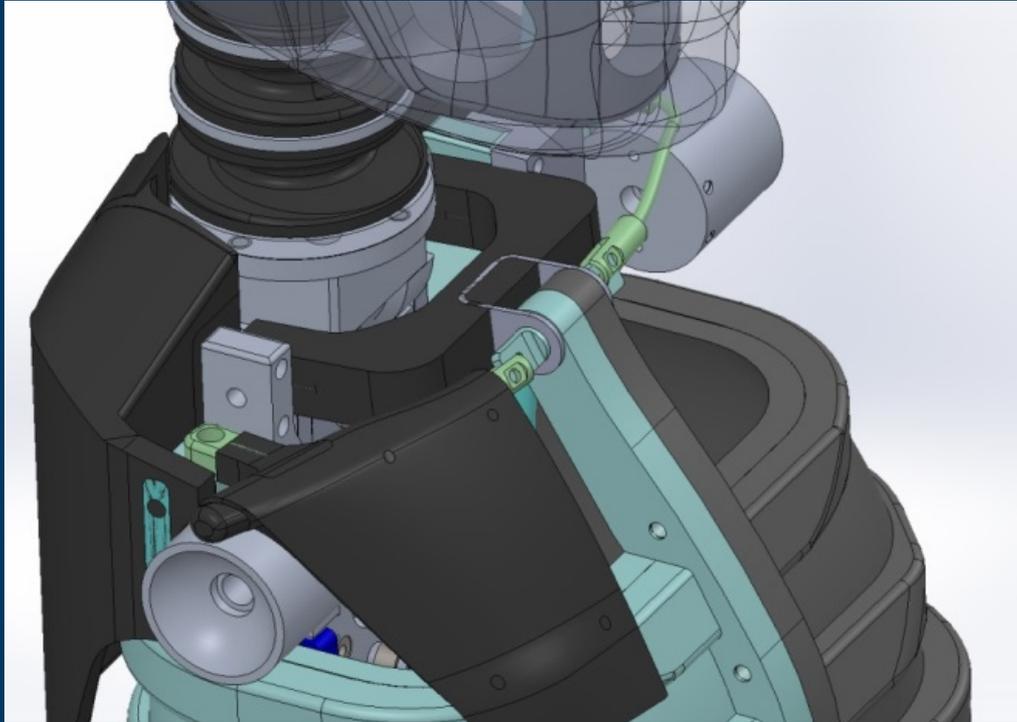


Positive chest deflection in 5 pt harness case resulting from harness spanning chest between shoulder and pelvis

60 – 80 mm of chest deflection is high; reinforcement of shoulders necessary to reduce loading of chest

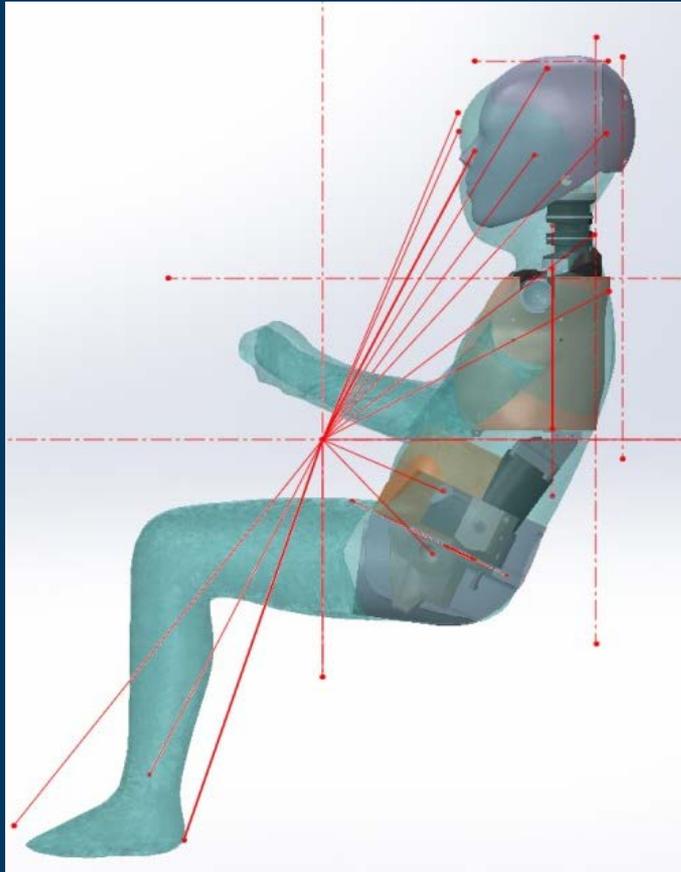
# Rev3: Shoulder Modifications

Shoulder stiffener to reduce chest compressions; scapula can rotate in Z axis as well

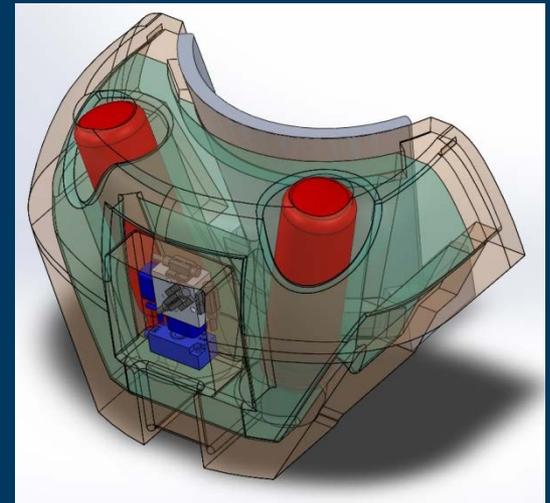
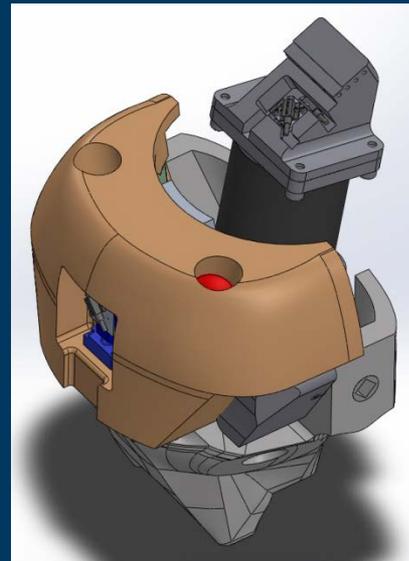
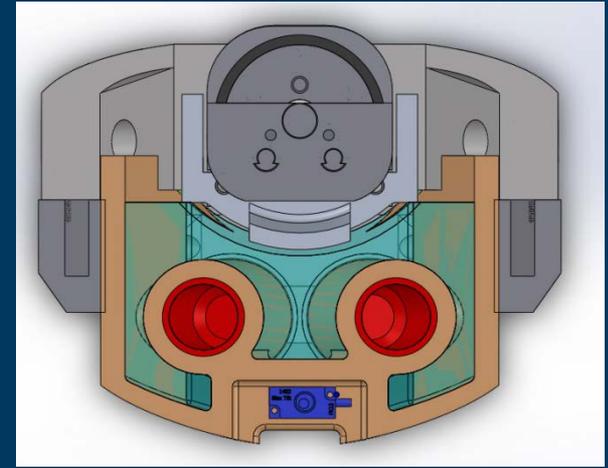
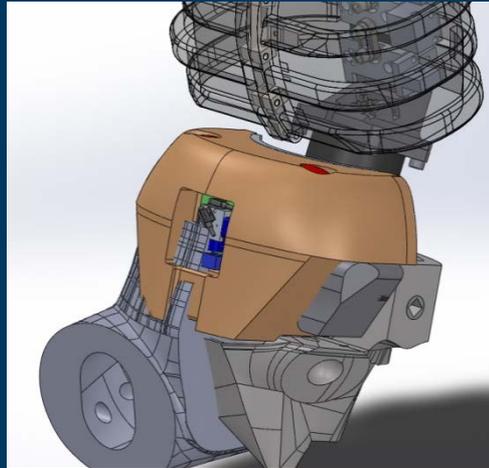


# Rev3: Abdomen & Pelvis Modifications

Added instrumentation & match UMTRI anthropometry



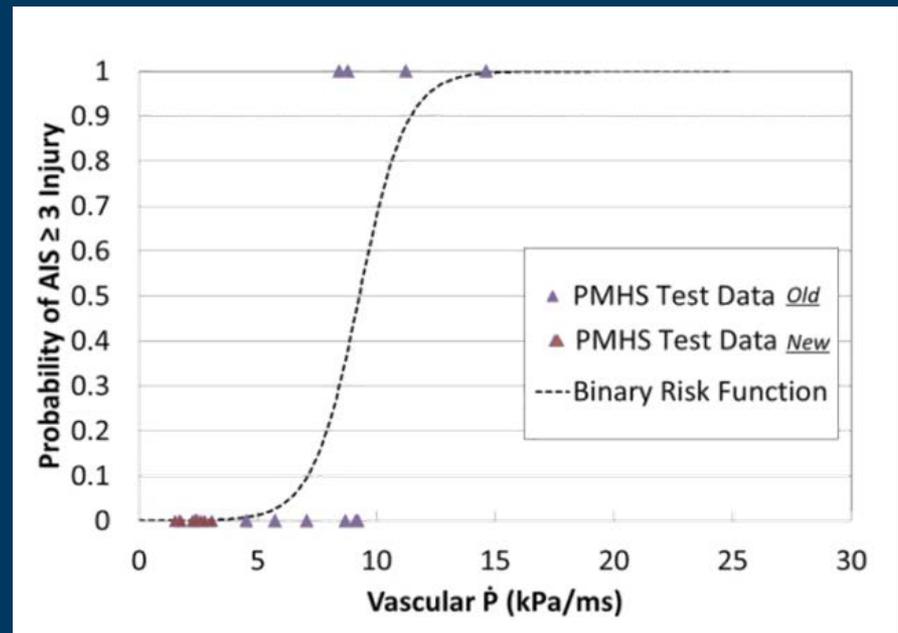
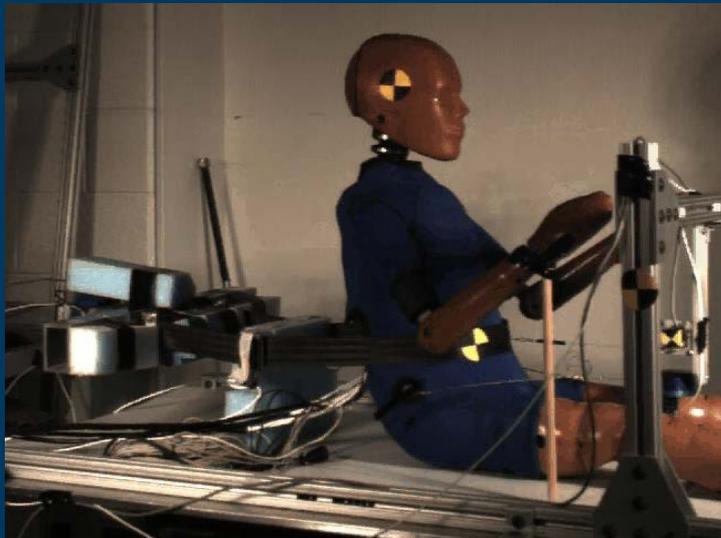
Anthropometry targets from [www.childshape.org](http://www.childshape.org) (UMTRI)



# Rev3: Abdomen Injury Assessment

Paired testing

- When F vs. d response biofidelity is sufficient, pressure and/or penetration based injury criteria can be derived for the LODC through paired testing with adult PMHS



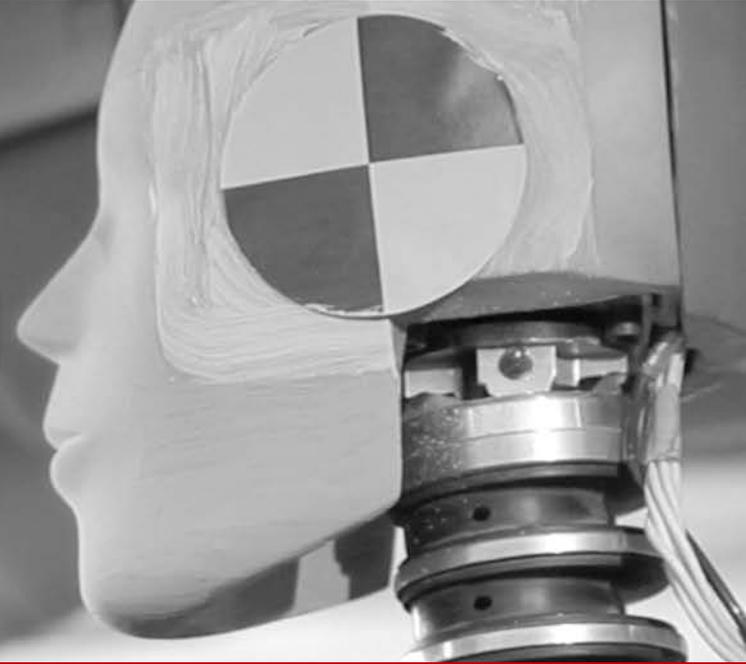
Injury risk functions from Kent et al (for penetration, Stapp 2008) and Kremer et al (for pressure rate, Stapp 2011)

# Summary

- Component responses match recent pediatric biomechanical data
- Improved head kinematics & reduced neck loads in FMVSS 213 environment
- High chest compressions require modifications to shoulder-ribcage interface
- Instrumented abdomen, humanlike pelvis geometry, and injury criteria will allow abdomen injury monitoring



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